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Automated radiosynthesis of two ^{18}F -labeled tracers containing 3-fluoro-2-hydroxypropyl moiety, [^{18}F]FMISO and [^{18}F]PM-PBB3, via [^{18}F]epifluorohydrin

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Abstract

Background: [^{18}F]Fluoromisonidazole ([^{18}F]FMISO) and 1-[^{18}F]fluoro-3-((2-((1*E*,3*E*)-4-(6-(methylamino)pyridine-3-yl)buta-1,3-dien-1-yl)benzo[d]thiazol-6-yl)oxy)propan-2-ol ([^{18}F]PM-PBB3 or [^{18}F]APN-1607) are clinically used radiotracers for imaging hypoxia and tau pathology, respectively. Both radiotracers were produced by direct ^{18}F -fluorination using the corresponding tosylate precursors 1 or 2 and [^{18}F]F⁻, followed by the removal of protecting groups. In this study, we synthesized [^{18}F]FMISO and [^{18}F]PM-PBB3 by ^{18}F -fluoroalkylation using [^{18}F]epifluorohydrin ([^{18}F]5) for clinical applications.

Results: First, [^{18}F]5 was synthesized by the reaction of 1,2-epoxypropyl tosylate (8) with [^{18}F]F⁻ and was purified by distillation. Subsequently, [^{18}F]5 was reacted with 2-nitroimidazole (6) or PBB3 (7) as a precursor for ^{18}F -labeling, and each reaction mixture was purified by preparative high-performance liquid chromatography and formulated to obtain the [^{18}F]FMISO or [^{18}F]PM-PBB3 injection. All synthetic sequences were performed using an automated ^{18}F -labeling synthesizer. The obtained [^{18}F]FMISO showed sufficient radioactivity (0.83 ± 0.20 GBq at the end of synthesis (EOS); $n = 8$) with appropriate radiochemical yield based on [^{18}F]F⁻ (26 ± 7.5 % at EOS, decay-corrected; $n = 8$). The obtained [^{18}F]PM-PBB3 also showed sufficient radioactivity (0.79 ± 0.10 GBq at EOS; $n = 11$) with appropriate radiochemical yield based on [^{18}F]F⁻ (16 ± 3.2 % at EOS, decay-corrected; $n = 11$).

Conclusions: Both [^{18}F]FMISO and [^{18}F]PM-PBB3 injections were successfully synthesized with sufficient radioactivity by ^{18}F -fluoroalkylation using [^{18}F]5.

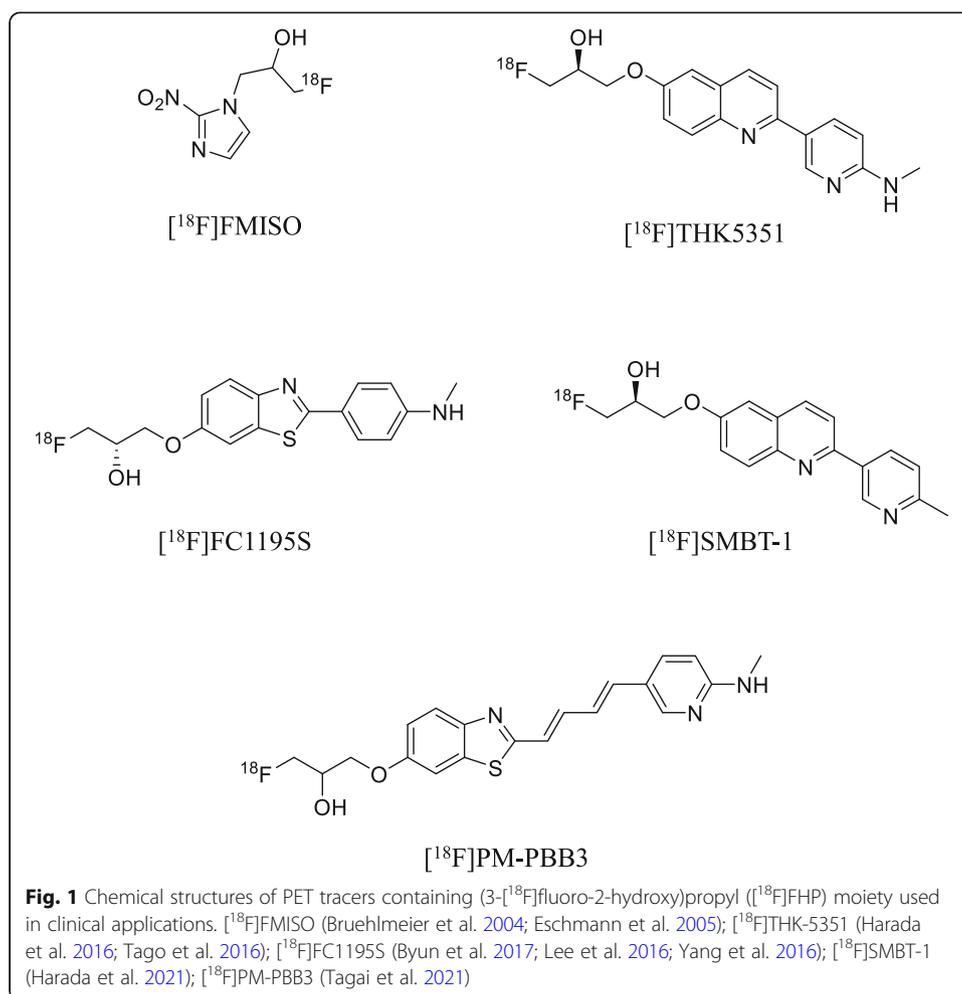
Keywords: ^{18}F , [^{18}F]Epifluorohydrin, [^{18}F]FMISO, [^{18}F]PM-PBB3, Positron emission tomography (PET)

Background

Fluorine-18 ($T_{1/2} = 109.8$ min) is indispensable for the development of positron emission tomography (PET) tracers because its decay characteristic is better than that of carbon-11 ($T_{1/2} = 20.1$ min). The direct ^{18}F -fluorination using a tosylate or triflate precursor and $[^{18}\text{F}]\text{F}^-$ is a widely used method for the introduction of fluorine-18 into target molecules to afford a large number of ^{18}F -labeled PET tracers (Cole et al. 2014; Deng et al. 2019; Miller et al. 2008). In addition, ^{18}F -fluoroalkylation is also a useful tool for inserting fluorine-18 into target molecules containing nucleophilic hydroxyl and amino functional groups (Zhang and Suzuki 2007). ^{18}F -Fluoroalkylation has some advantages over direct ^{18}F -fluorination. For example, ^{18}F -fluoroalkylation applies more accessible and available phenols, carboxylic acids, amines, and amides as precursors for ^{18}F -labeling (Iwata et al. 2002; Wilson et al. 1995; Zhang and Suzuki 2007). We have synthesized ^{18}F -fluoroalkyl agents, such as $[^{18}\text{F}]$ fluoro-methyl, ethyl, and propyl bromide ($[^{18}\text{F}]\text{F}(\text{CH}_2)_n\text{Br}$, $n = 1-3$) (Yanamoto et al. 2009; Yui et al. 2010; Zhang et al. 2002, 2003, 2004; Zhang and Suzuki 2007), deuterium-substituted $[^{18}\text{F}]$ fluoromethyl bromide ($[^{18}\text{F}]\text{FCD}_2\text{Br}$), and its triflate ($[^{18}\text{F}]\text{FCD}_2\text{OTf}$) using an automated ^{18}F -labeling synthesizer (Arakawa et al. 2008; Mori et al. 2019). Using these ^{18}F -fluoroalkyl agents, we synthesized dozens of ^{18}F -fluoroalkylated tracers starting from the precursors of phenols, carboxylic acids, amines, and amides for PET imaging of receptors, enzymes, and transporters in the brain (Zhang and Suzuki 2007). Among these PET tracers, $[^{18}\text{F}]\text{FEDAA1106}$ (Fujimura et al. 2006), $[^{18}\text{F}]\text{FE-SPARQ}$ (Haneda et al. 2007), $[^{18}\text{F}]\text{FMeNER-}d_2$ (Arakawa et al. 2008), $[^{18}\text{F}]\text{FEPE2I}$ (Sasaki et al. 2012), and $[^{18}\text{F}]\text{FEDAC}$ (Chung et al. 2018; Xie et al. 2012) have been synthesized for clinical applications in our PET center.

The ^{18}F -3-fluoro-2-hydroxypropyl (^{18}F -FHP) moiety was used instead of the aforementioned conventional ^{18}F -fluoroalkyl moieties. Many PET tracers containing the ^{18}F -FHP moiety have been developed, some of which have been used in clinical studies, such as $[^{18}\text{F}]\text{FMISO}$ (Bruehlmeier et al. 2004; Eschmann et al. 2005), $[^{18}\text{F}]\text{THK-5351}$ (Harada et al. 2016; Tago et al. 2016), $[^{18}\text{F}]\text{FC1195S}$ (Byun et al. 2017; Lee et al. 2016; Yang et al. 2016), $[^{18}\text{F}]\text{SMBT-1}$ (Harada et al. 2021), and $[^{18}\text{F}]\text{PM-PBB3}$ (Tagai et al. 2021; Kawamura et al. 2021) (Fig. 1). Among these PET tracers, $[^{18}\text{F}]\text{THK-5351}$ (Fig. 1), which contains the FHP moiety, showed improved *in vivo* metabolic stability compared with its fluoropropyl analog (Tago et al. 2016).

To date, many ^{18}F -labeled tracers containing ^{18}F -fluoroalkyl moieties have been developed. To synthesize these PET tracers, direct ^{18}F -fluorination of the corresponding tosylate or triflate precursor with $[^{18}\text{F}]\text{F}^-$ is a conventional method. Among these, $[^{18}\text{F}]\text{FMISO}$ as a PET imaging agent for tumor hypoxia (Oh et al. 2005; Tang et al. 2005), and $[^{18}\text{F}]\text{PM-PBB3}$ as a PET imaging agent for tau pathology (Kawamura et al. 2021) have been prepared by direct ^{18}F -fluorination using tosylate precursors and $[^{18}\text{F}]\text{F}^-$, followed by the removal of the protecting group. The direct ^{18}F -fluorination was achieved within the same reaction vessel using an automated synthesizer. Moreover, the one-step radiolabeling technique for ^{18}F -labeled tracers could be readily transferred to other PET centers for multisite studies using the same study protocol (Kawamura et al. 2016, 2021; Mori et al. 2017). In fact, automated radiosynthesis of $[^{18}\text{F}]\text{PM-PBB3}$ by direct ^{18}F -fluorination has been transferred to a dozen PET centers in Japan, China, Taiwan, and the USA (Hsu et al. 2020; Su et al. 2020; Weng et al.



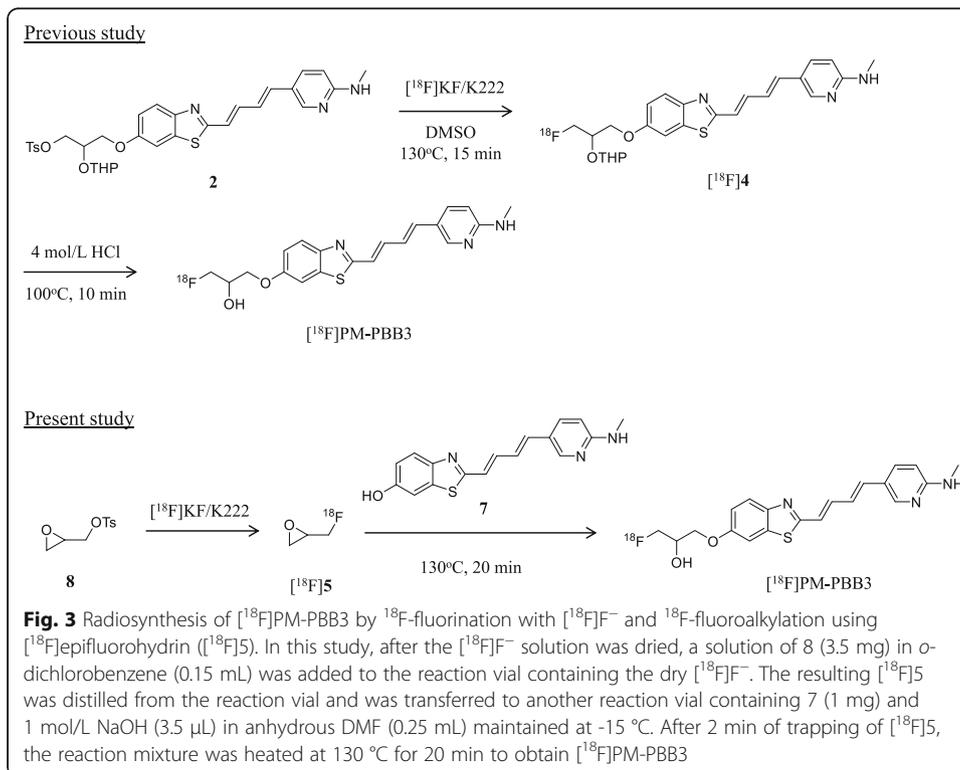
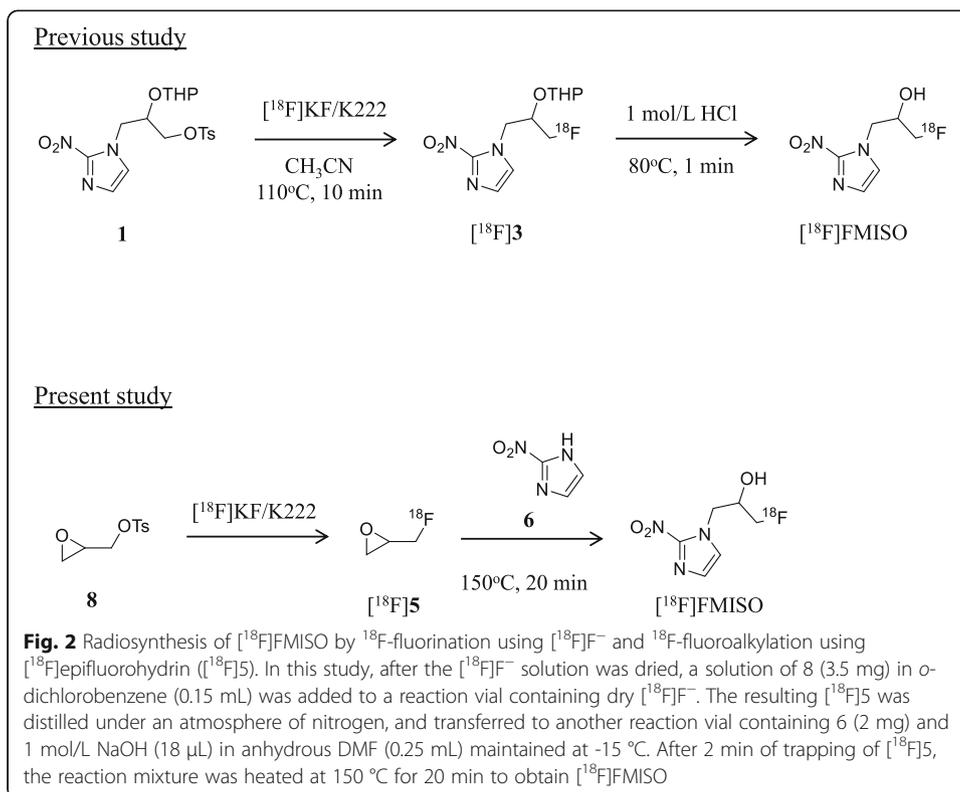
2020). As for the limitation of these direct ^{18}F -fluorination, it is noted that tosylated precursors should be synthesized in at least two steps. ^{18}F FMISO was synthesized using ^{18}F epfluorohydrin (^{18}F 5), as described previously (Grierson et al. 1989; Kämäräinen et al. 2004; McCarthy et al. 1993). In those papers, fully automated radiosynthesis procedures of ^{18}F FMISO via ^{18}F 5 using an ^{18}F -labeling synthesizer have not been reported.

In this study, to determine an effective synthetic route for ^{18}F FMISO and ^{18}F PM-PBB3 with sufficient radioactivity and high quality for clinical applications, we synthesized the two PET tracers using ^{18}F 5 as an ^{18}F -labeling agent by the reaction of easily accessible 2-nitroimidazole (6, Fig. 2) or PBB3 (a phenol precursor; 7, Fig. 3) using an ^{18}F -labeling synthesizer equipped with a fully automated system. Furthermore, we compared the synthetic results of ^{18}F -fluoroalkylation using ^{18}F 5 and ^{18}F -fluorination using $^{18}\text{F}\text{F}^-$ to evaluate their relative merits.

Methods

General

1 *H*-1-(3-Fluoro-2-hydroxypropyl)-2-nitroimidazole (FMISO, Fig. 1) and 2-nitroimidazole (6, Fig. 2) were purchased from ABX (Radeberg, Germany). 1-Fluoro-3-



((2-((1*E*,3*E*)-4-(6-(methylamino)pyridine-3-yl)buta-1,3-dien-1-yl)benzo[*d*]thiazol-6-yl)oxy)propan-2-ol (PM-PBB3, Fig. 1), and 2-((1*E*,3*E*)-4-(6-(methylamino)pyridin-3-yl)buta-1,3-dienyl)benzo[*d*]thiazol-6-ol (PBB3; 7, Fig. 3) (Hashimoto et al. 2014; Maruyama et al. 2013) were provided by Shanghai ChemPartner (Shanghai, China). All chemical reagents and organic solvents were purchased from Sigma-Aldrich (St. Louis, MO, USA), Fujifilm Wako Pure Chemical Co. (Osaka, Japan), and Nacalai Tesque (Kyoto, Japan), and were used without any further purification. Fluorine-18 was produced by the $^{18}\text{O}(p, n)^{18}\text{F}$ nuclear reaction using a CYPRIIS HM-18 cyclotron (Sumitomo Heavy Industry, Tokyo, Japan). A dose calibrator (IGC-3R Curiometer; Aloka, Tokyo, Japan) was used for all radioactivity measurements, unless otherwise stated. An automated multi-purpose synthesizer developed in-house was used for all the radiosynthetic runs in this study (Supplemental information: Fig. S1, Fukumura et al. 2007). Preparative high-performance liquid chromatography (HPLC) was performed using a JASCO HPLC system (PU-2080 pump and UV-2075 detector; JASCO, Tokyo, Japan) equipped with a radioactivity detector (Ohyo Koken Kogyo, Tokyo, Japan). All radiochemical yields were decay-corrected to the end of synthesis. Fluorine-18, as $[^{18}\text{F}]\text{F}^-$, was produced as described previously (Fujinaga et al. 2018).

Automated radiosynthesis of $[^{18}\text{F}]\text{FMISO}$ using $[^{18}\text{F}]\text{5}$

After the $[^{18}\text{F}]\text{F}^-$ solution (5.2 ± 0.20 GBq, $n = 8$) was dried, a solution of epoxypropyl tosylate (**8**, 3.5 mg) in *o*-dichlorobenzene (0.15 mL) was added to the reaction vial containing dry $[^{18}\text{F}]\text{F}^-$ at 130 °C. The resulting $[^{18}\text{F}]\text{5}$ was distilled from the reaction vial under N_2 flow at 30 mL/min and was transferred to another reaction vial containing precursor **6** (2 mg) and 1 mol/L sodium hydroxide solution (NaOH, 18 μL) in anhydrous *N,N*-dimethylformamide (DMF, 0.25 mL) maintained at -15 °C. After 2 min of trapping of $[^{18}\text{F}]\text{5}$, the reaction mixture was heated at 150 °C for 20 min, and then was diluted with the preparative HPLC eluent (0.5 mL). The solution mixture was transferred to the injector for preparative HPLC, as described in the [general](#) section. The HPLC conditions were as follows: XBridge C_{18} column (5 μm , 10 mm i.d. \times 250 mm length; Waters), a mixture of ethanol and water (2:98, vol./vol.) as the mobile phase, 5.0 mL/min flow rate, and UV detection at 325 nm. The retention time of $[^{18}\text{F}]\text{FMISO}$ was approximately 12 min. The HPLC fraction of $[^{18}\text{F}]\text{FMISO}$ was collected in a flask containing polysorbate 80 (75 μL) in ethanol (0.3 mL), and ascorbic acid for injection (25 mg/0.1 mL water) was added before radiosynthesis. The solution was subsequently evaporated to dryness, and the residue was dissolved in physiological saline (3–10 mL). The resulting solution was passed through a Millex-GV filter (Millipore) to obtain $[^{18}\text{F}]\text{FMISO}$ as an injectable solution.

The radiochemical purity of $[^{18}\text{F}]\text{FMISO}$ was determined using analytical HPLC under the following conditions: XBridge C_{18} column (5 μm , 4.6 mm i.d. \times 150 mm length; Waters), a mixture of 90 % acetonitrile solution and 50 mM ammonium phosphate buffer (pH 9.3) (7:93, vol./vol.) as the mobile phase, 1.0 mL/min flow rate, and UV detection at 325 nm. The retention time of $[^{18}\text{F}]\text{FMISO}$ was 5.6 min. The identity of $[^{18}\text{F}]\text{FMISO}$ was confirmed by co-injecting it with authentic unlabeled FMISO. The molar activity of $[^{18}\text{F}]\text{FMISO}$ was measured using the same analytical HPLC system. The mass (μmol) of FMISO with a known

radioactivity (GBq) was determined using analytical HPLC by comparing the UV absorbance at 325 nm of [^{18}F]FMISO with that of known concentrations of unlabeled FMISO.

Automated radiosynthesis of [^{18}F]PM-PBB3 using [^{18}F]5

After the [^{18}F]F $^-$ solution (7.4 ± 0.20 GBq, $n = 11$) was dried, a solution of epoxypropyl tosylate (**8**, 3.5 mg) in *o*-dichlorobenzene (0.15 mL) was added automatically to the reaction vial containing the dry [^{18}F]F $^-$ at 130 °C. The resulting [^{18}F]5 was distilled from the reaction vial under N $_2$ flow at 30 mL/min and was transferred to another reaction vial containing precursor **7** (1 mg) and 1 mol/L NaOH (3.5 μL) in anhydrous DMF (0.25 mL) maintained at -15 °C. After 2 min of trapping of [^{18}F]5, the reaction mixture was heated at 130 °C for 20 min, and then was diluted with the preparative HPLC eluent (0.5 mL). The solution was transferred to the injector for preparative HPLC, as described in the [general](#) section. The HPLC conditions were as follows: Capcell Pak C $_{18}$ column (5 μm , 10 mm i.d. \times 250 mm length; Shiseido, Tokyo, Japan), a mixture of acetonitrile, water, and triethylamine (40:60:0.1, vol./vol./vol.) as the mobile phase, 5.0 mL/min flow rate, and UV detection at 365 nm. The retention time of [^{18}F]PM-PBB3 was 14.9 min. The HPLC fraction of [^{18}F]PM-PBB3 was collected in a flask containing polysorbate 80 (75 μL) in ethanol (0.3 mL) and ascorbic acid for injection (25 mg/0.1 mL water) was added before radiosynthesis. The solution was subsequently evaporated to dryness, and the residue was dissolved in physiological saline (3–10 mL). The solution of [^{18}F]PM-PBB3 was passed through a Millex-GV filter to obtain [^{18}F]PM-PBB3 as an injectable solution. The preparative HPLC and formulation were performed under UV-cut light (< 500 nm wavelength cutoff, ECOHiLUX HES-YF; Iris Oyama, Sendai, Japan) to prevent the photoisomerization of [^{18}F]PM-PBB3, because [^{18}F]PM-PBB3 underwent rapid photoisomerization upon exposure to fluorescent light (Kawamura et al. 2021).

The radiochemical purity of [^{18}F]PM-PBB3 was determined by analytical HPLC under the following conditions: Atlantis T3 column (5 μm , 4.6 mm i.d. \times 150 mm length; Waters), a mixture of acetonitrile and 50 mM ammonium acetate (pH 6.5) (40:60, vol./vol.) as the mobile phase, 1.0 mL/min flow rate, and UV detection at 365 nm. The retention time of [^{18}F]PM-PBB3 was 12 min. The identity of [^{18}F]PM-PBB3 was confirmed by co-injecting it with authentic unlabeled PM-PBB3. The molar activity of [^{18}F]PM-PBB3 was measured using the same analytical HPLC system. The mass (μmol) of [^{18}F]PM-PBB3 with a known radioactivity (GBq) was determined by comparing the UV absorbance at 365 nm of PM-PBB3 with that of known concentrations of unlabeled PM-PBB3. All of the above analytical processes were conducted in the absence of fluorescent light to prevent the photoisomerization of [^{18}F]PM-PBB3.

Results

Automated radiosynthesis of [^{18}F]FMISO using [^{18}F]5

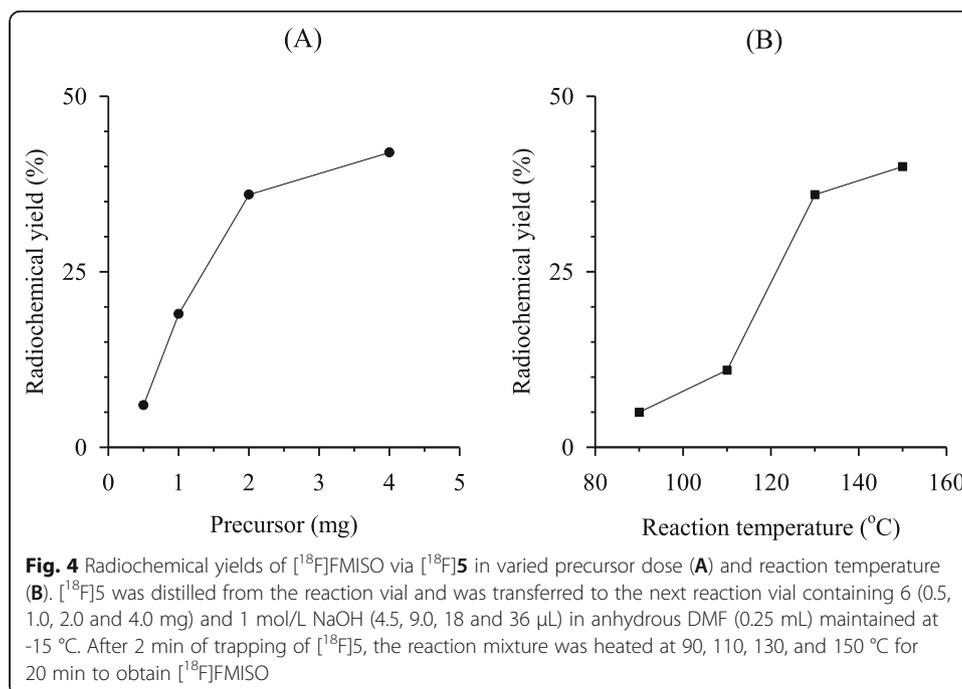
We synthesized [^{18}F]FMISO under various reaction conditions for the ^{18}F -fluoroalkylation of 2-nitroimidazole precursor **6** and [^{18}F]5 using an automated ^{18}F -labeling synthesizer. With an increase in the amount of **6** from 0.5 to 4 mg, the radiochemical yield of [^{18}F]FMISO gradually increased to 36% from 0.5 to 2 mg, and marginally

increased up to 42 % from 2 to 4 mg [Fig. 4(A)]. In addition, increasing the reaction temperature from 90 to 150 °C increased the radiochemical yield of [^{18}F]FMISO by up to 40 % [Fig. 4(B)]. Furthermore, the radiochemical yield obtained by using sodium hydroxide (36 %) as a base for the reaction was slightly higher than that obtained by using sodium carbonate (22 %) or potassium hydroxide (24 %). From these results, we optimized the conditions for the radiosynthesis of [^{18}F]FMISO using [^{18}F]5 as follows: 2 mg of precursor 6, 18 μmol of sodium hydroxide as a base for the reaction, and a reaction temperature of 150 °C for 20 min. After completion of the reaction, preparative HPLC for the reaction mixture was performed to efficiently separate [^{18}F]FMISO from the mixture, affording the radiochemically and chemically pure product as an injectable solution [Fig. 5(A)]. No significant UV peak corresponding to unreacted 6 and its decomposition components were observed in the analytical HPLC chromatogram of the final product solution [Fig. 5(B)].

Table 1 summarizes the results of the automated radiosynthesis of [^{18}F]FMISO by ^{18}F -fluoroalkylation using 6 and [^{18}F]5 for clinical applications. We successfully synthesized [^{18}F]FMISO using [^{18}F]5, with sufficient radioactivity (0.83 ± 0.2 GBq, $n = 8$) for clinical applications. The radiochemical yield of [^{18}F]FMISO based on the cyclotron-produced [^{18}F]F $^-$ at the end of the synthesis (EOS) was 26 ± 7.5 % ($n = 8$). All the results of quality control for the [^{18}F]FMISO injection complied with our in-house quality control and quality assurance specifications (Table 1).

Automated radiosynthesis of [^{18}F]PM-PBB3 using [^{18}F]5

We synthesized [^{18}F]PM-PBB3 by the ^{18}F -fluoroalkylation of precursor 7 and [^{18}F]5 (Fig. 3), according to the reaction conditions previously determined for the reaction of



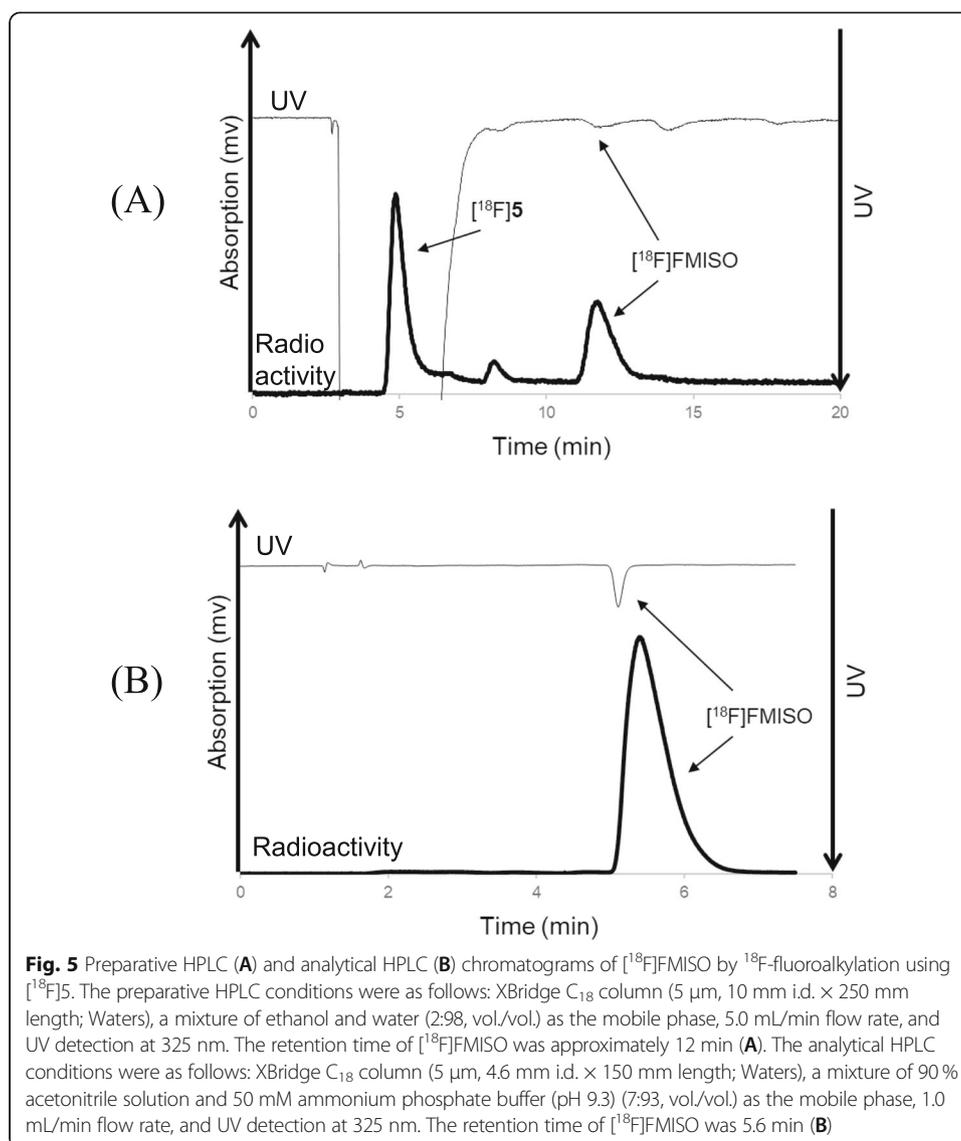


Table 1 Radiosynthesis results of $[^{18}\text{F}]$ FMISO and $[^{18}\text{F}]$ PM-PBB3 by ^{18}F -fluoroalkylation using precursor 6 and $[^{18}\text{F}]$ 5

	$[^{18}\text{F}]$ FMISO	$[^{18}\text{F}]$ PM-PBB3
Cyclotron-produced $[^{18}\text{F}]\text{F}^-$ (GBq)	$5.2 \pm 0.20^{\text{b}}$	$7.4 \pm 0.20^{\text{d}}$
Radioactivity (GBq) ^a	$0.83 \pm 0.20^{\text{b}}$	$0.79 \pm 0.10^{\text{d}}$
Radiochemical yield (%) ^a	$26 \pm 7.5^{\text{b}}$ (40 ^c)	$16 \pm 3.2^{\text{d}}$ (25 \pm 6.0 ^e)
Radiochemical purity (%)		
EOS	$99 \pm 0.50^{\text{b}}$	$99 \pm 0.50^{\text{d}}$
3 h after EOS	$> 95^{\text{c}}$	$> 95^{\text{d}}$
Synthesis time (min)	$75 \pm 4.0^{\text{b}}$	$78 \pm 4.0^{\text{d}}$
Molar activity (GBq/ μmol) ^a	$110 \pm 20^{\text{c}}$	$330 \pm 140^{\text{d}}$

^aAt the end of synthesis (EOS)

^b $n = 8$

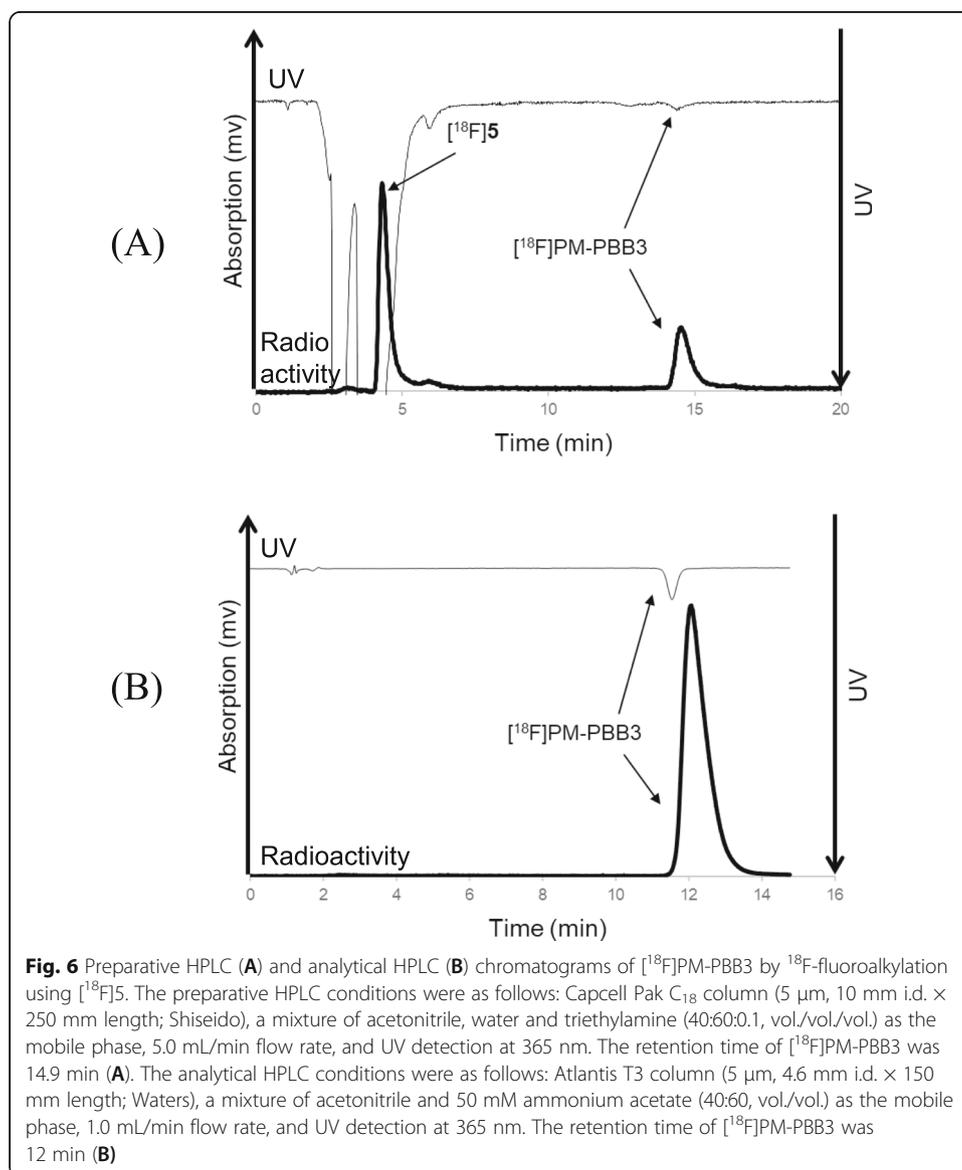
^cthe average result using ^{18}F -fluorination in our routine radiosynthesis

^d $n = 11$

^ethe result using ^{18}F -fluorination ($n = 53$) (Kawamura et al. 2021)

a conventional phenol precursor with [^{18}F]5 (Fujinaga et al. 2018). After the trapping of [^{18}F]5 for 2 min, the ^{18}F -fluoroalkylation of 7 and [^{18}F]5 was performed at 130 °C for 20 min. The reaction mixture was then separated using preparative HPLC [Fig. 6(A)] to produce radiochemically and chemically pure [^{18}F]PM-PBB3 as an injectable solution [Fig. 6(B)].

Table 1 summarizes the automated radiosynthesis results of [^{18}F]PM-PBB3 by ^{18}F -fluoroalkylation using precursor 7 and [^{18}F]5 for clinical applications. We successfully synthesized [^{18}F]PM-PBB3 using [^{18}F]5, with sufficient radioactivity (0.79 ± 0.1 GBq, $n = 11$) for clinical applications. In addition, the radiochemical yield of [^{18}F]PM-PBB3 based on the cyclotron-produced [^{18}F]F $^-$ at EOS was $16 \pm 3.2\%$ ($n = 11$). All the results of quality control for the [^{18}F]PM-PBB3 injection complied with our in-house quality control and quality assurance specifications (Table 1).



Discussion

We successfully synthesized [^{18}F]FMISO and [^{18}F]PM-PBB3 by ^{18}F -fluoroalkylation using [^{18}F]5 with sufficient radioactivity for clinical applications. For [^{18}F]FMISO, the radiochemical yield of the ^{18}F -fluoroalkylation of 6 with [^{18}F]5 was $26 \pm 7.5\%$ ($n = 8$, Table 1), while the yield by the direct ^{18}F -fluorination of 1 with [^{18}F]F $^-$ was approximately 40% (from the average result in our routine radiosynthesis). For [^{18}F]PM-PBB3, the radiochemical yield of the ^{18}F -fluoroalkylation of 7 with [^{18}F]5 was $16 \pm 3.2\%$ ($n = 11$, Table 1), whereas the yield obtained by the direct ^{18}F -fluorination of 2 with [^{18}F]F $^-$ was $25 \pm 6.0\%$ ($n = 53$) (Kawamura et al. 2021). The reason for the difference in radiochemical yields between the two methods is the relatively lower reactivity of the corresponding precursors toward [^{18}F]5 as a radiolabeling agent than toward [^{18}F]F $^-$. Moreover, the reactivity of [^{18}F]5 seemed to be lower than that of conventional ^{18}F -fluoroalkyl agents, such as [^{18}F]fluoroethyl bromide and [^{18}F]fluoroethyl iodide, toward the same phenol precursor. Recently, we found that the use of some Lewis acids could increase the reactivity of [^{18}F]5 with aniline analogs (Fujinaga et al. 2019) and expect that the radiochemical yield of PET tracers containing the ^{18}F -FHP moiety could be increased by ^{18}F -fluoroalkylation using phenol or amine and [^{18}F]5, catalyzed by a Lewis acid.

On the other hand, for direct ^{18}F -fluorination, the tosylate precursors 1 and 2 should be synthesized with at least two steps from 6 to 7, respectively, and were limited to only the radiosynthesis of [^{18}F]FMISO and [^{18}F]PM-PBB3. For ^{18}F -fluoroalkylation, imidazole precursor 6 and phenol precursor 7 are available and accessible. In particular, precursor 7 (PBB3) is an authentic unlabeled compound of [^{11}C]PBB3, which is a clinically used radiotracer for PET imaging of tauopathy in the human brain (Hashimoto et al. 2014, 2015; Maruyama et al. 2013). Moreover, 6 or 7 could be used to react with [^{18}F]5 as well as other radiolabeling agents, such as [^{11}C]methyl iodide and ^{18}F -fluoroalkyl agents, to produce diverse PET tracer candidates. A structure-activity relationship study is helpful for finding PET tracers with improved *in vitro* properties and *in vivo* behaviors by reacting the same precursor with diverse radiolabeling agents. This strategy has been applied to develop PET tracers in our group and to explore the best version from a series of candidates with the same chemical skeleton (Fujinaga et al. 2012; Zhang et al. 2003, 2004).

In this synthesis, the resulting [^{18}F]5 radiolabeling agent was purified by distillation from an ^{18}F -fluorinated mixture of epoxytosylate 8 with [^{18}F]F $^-$, and was used for ^{18}F -fluoroalkylation (Fujinaga et al. 2018). The distillation procedure removed all non-volatile impurities, such as metal ions from the cyclotron target, unreacted 8 and [^{18}F]F $^-$, and the phase transfer reagent Kryptofix 222 and K_2CO_3 . Because of the utilization of purified [^{18}F]5, only a small amount of precursor 6 (2 mg) or 7 (1 mg) was used for the ^{18}F -fluoroalkylation, resulting in a clear ^{18}F -fluoroalkylated reaction mixture. As shown in the respective HPLC separation charts for the reaction mixtures, in addition to the unreacted [^{18}F]5, only the desired product corresponding to [^{18}F]FMISO [Fig. 5(A)] or [^{18}F]PM-PBB3 [Fig. 6(A)] peak was obtained from the reaction. Because of the large difference in the retention times of [^{18}F]5 and [^{18}F]FMISO or [^{18}F]PM-PBB3, HPLC separation was easily conducted to obtain two radiochemically and chemically pure products [Fig. 5(B) and 6(B)]. Moreover, after ^{18}F -fluoroalkylation, the reaction mixture did not require deprotection with acid, directly resulting in [^{18}F]FMISO or [^{18}F]PM-PBB3.

For direct ^{18}F -fluorination, the tosylate precursor 1 or 2 is not stable in the presence of excess K_2CO_3 and Kryptofix 222 at high temperatures; therefore, a relatively large amount of 1 (5 mg) (Tang et al. 2005) or 2 (2 mg) (Kawamura et al. 2021) was required for the ^{18}F -fluorination with $[^{18}\text{F}]\text{F}^-$ in order to produce sufficient radioactivity for clinical applications. The unreacted precursors and decomposed chemical components made the HPLC purification inconvenient (Supplemental information: Fig. S2 and S3). In the synthesis of $[^{18}\text{F}]\text{FMISO}$ by the ^{18}F -fluorination using 1 and $[^{18}\text{F}]\text{F}^-$, after removal of the tosyl group in $[^{18}\text{F}]\text{3}$ by treating the reaction mixture with HCl, *p*-toluenesulfonic acid (TsOH) was obtained. Only HPLC separation of the reaction mixture could not remove TsOH perfectly, and part of it would be left in the final product solution. Therefore, in our laboratory, after preparative HPLC for the reaction mixture of $[^{18}\text{F}]\text{3}$ with HCl, the HPLC fraction was passed through a Sep-Pak cartridge (Cl^- form) to remove TsOH. In addition, $[^{18}\text{F}]\text{FMISO}$ was obtained as a chemically and radiochemically pure injectable solution.

Conclusions

In this study, we successfully synthesized $[^{18}\text{F}]\text{FMISO}$ and $[^{18}\text{F}]\text{PM-PBB3}$ by the ^{18}F -fluoroalkylation using $[^{18}\text{F}]\text{5}$, although the radiochemical yields of the ^{18}F -fluoroalkylation using $[^{18}\text{F}]\text{5}$ were relatively lower than those of the corresponding direct ^{18}F -fluorination using $[^{18}\text{F}]\text{F}^-$. Although the radiochemical yields were slightly lower for the synthesis route, the ^{18}F -fluoroalkylations with $[^{18}\text{F}]\text{5}$ were cleaner and thus purification by HPLC alone yielded very pure products. Furthermore, we obtained relatively high chemical and radiochemical purity of $[^{18}\text{F}]\text{FMISO}$ or $[^{18}\text{F}]\text{PM-PBB3}$ injection by radiosynthesis with the ^{18}F -fluoroalkylation using $[^{18}\text{F}]\text{5}$. Radiosynthesis using $[^{18}\text{F}]\text{5}$ is expected to be widely used to develop and produce useful PET tracers containing the ^{18}F -FHP moiety.

Abbreviations

$[^{18}\text{F}]\text{FMISO}$: $[^{18}\text{F}]\text{Fluoromisonidazole}$; $[^{18}\text{F}]\text{PM-PBB3}$: 1- $[^{18}\text{F}]\text{Fluoro-3-}((2-((1E,3E)-4-(6-(methylamino)pyridine-3-yl)buta-1,3-dien-1-yl)benzo[d]thiazol-6-yl)oxy)propan-2-ol$; $[^{18}\text{F}]\text{5}$: $[^{18}\text{F}]\text{Epifluorohydrin}$; HPLC: High-performance liquid chromatography; PET: Positron emission tomography; ^{18}F -FHP: ^{18}F -3-Fluoro-2-hydroxypropyl; PBB3: 2- $((1E,3E)-4-(6-(methylamino)pyridin-3-yl)buta-1,3-dienyl)benzo[d]thiazol-6-ol$; K_2CO_3 : Potassium carbonate; Kryptofix 222: 4,7,13,16,21,24-Hexaoxa-1,10-diazabicyclo[8,8,8]hexacosane; CH_3CN : Acetonitrile; NaOH: Sodium hydroxide; DMF: *N,N*-Dimethylformamide; TsOH: *p*-Toluenesulfonic acid; EOS: The end of synthesis

Supplementary Information

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Additional file 1: Figure S1. The system diagram of automated multi-purpose synthesizer developed in-house (Fukumura et al. 2007). **Figure S2.** The preparative HPLC chromatogram of $[^{18}\text{F}]\text{FMISO}$ synthesized by ^{18}F -fluorination using 1 and $[^{18}\text{F}]\text{F}^-$, followed by the removal of the protecting group in $[^{18}\text{F}]\text{3}$. The HPLC conditions were as follows: XBridge C18 column (5 μm , 10 mm i.d. \times 250 mm length; Waters), with a mixture of ethanol and water (2:98, vol./vol.) as the mobile phase, a flow rate of 5.0 mL/min, and UV detection at 325 nm. **Figure S3.** The preparative HPLC chromatograms of $[^{18}\text{F}]\text{PM-PBB3}$ synthesized by ^{18}F -fluorination using 2 and $[^{18}\text{F}]\text{F}^-$, followed by the removal of the protecting group in $[^{18}\text{F}]\text{4}$. The HPLC conditions were as follows: Capcell Pak C18 column (5 μm , 10 mm i.d. \times 250 mm length; Shiseido, Tokyo, Japan), the mixture of acetonitrile, water and triethylamine (40:60:0.1, v/v) as the mobile phase, 5.0 mL/min flow rate, and UV detection at 365 nm.

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Authors' contributions

TO designed the study, performed synthesis, and analyzed the data; YK, MO, and NN operated the radiosynthesizer; MF, WM, KK, and MH assisted with the synthesis; KF and HH analyzed the quality control data; KK summarized the study, and wrote the manuscript; MRZ designed the study and reviewed the manuscript; all authors read and approved the final manuscript.

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Availability of data and materials

Data are provided in the article and supplementary information.

Declarations

Ethics approval and consent to participate

Not applicable.

Consent for publication

Not applicable.

Competing interests

The authors declare no potential conflicts of interest with respect to the authorship or publication of this article.

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